

Effect of Different Air Hole Diameters of the Inspiratory Muscle Trainer on the Rating of Perceived Exertion and Inspiratory Muscle Activity during Breathing Exercise

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Abstract

Purpose : This study aims to investigate the rating of perceived exertion (RPE) and muscle activity of the inspiratory primary and accessory muscle during breathing exercise with different air hole diameters of the inspiratory muscle trainer (IMT).

Methods : The Borg's scale and surface electromyography (EMG) was used to collect data of the RPE and muscle activity of the inspiratory primary the external intercostal (EI) and diaphragm (DIA) and accessory muscles anterior scalene (AS), sternocleidomastoid (SCM), pectoralis major (PM), and upper trapezius (UT) muscles during breathing exercise with different air hole diameters (6 mm, 4 mm, and 2 mm) of the IMT in healthy young male subjects.

Results : The RPE and muscle activities of the AS, SCM, and UT are increased significantly in accordance to the decreasing diameter of air hole of air tip in IMT. However, there are no differences in the muscle activities of the PM, EI, and DIA based on differences of diameters of air hole of air tip in IMT.

Conclusion : The smaller the diameter of IMT air-hole, RPE and muscle activities of AS, SCM and UT were increased. Therefore, further study would be necessary to investigate the proper intensity and relaxation posture for the exercise protocol to strengthen the inspiratory primary muscles.

Key Words : different diameters of air tip of inspiratory muscle trainer, inspiratory primary and accessory muscle, muscle activity, rating of perceived exertion

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I . Introduction

1. Background

Pulmonary diseases were classified as obstructive, restrictive, and other diseases (Watanabe et al., 2018). Among the intervention methods performed for pulmonary rehabilitation, the inspiratory muscle trainer (IMT) developed for strengthening the inspiratory muscle of the patient has various types of resistance (Beaumont et al., 2018). According to the resistance method, the IMT were divided into a method of changing the air hole diameter of the air tip, a method of using elasticity of the spring, and a buoyancy device using the sound pressure in the exercise device (Lin et al., 2012). IMT device which was controlled through the size of the air hole diameter, has 6 different hole diameter size of the air tip ranging from 2 mm to 7 mm.

IMT increased inspiratory muscle capacity, and improved exercise tolerance and perception of breathlessness during activities of daily living (Gosselink et al., 2011). Breathing exercise using IMT was usually applied once for 15~30 minutes, twice or three times a day, and the choice of the hole diameter size of the air tip to determine the resistance depends on the tolerance of the patient (Johnson et al., 1998). However, breathing exercises for strengthening inspiratory muscles often caused pain of trunk muscles and dyspnea. Pain and dyspnea during inspiratory muscle strengthening exercise can be considered as fatigue caused by overload due to resistance exceeding tolerance and exercise capacity of patient (Enoka & Duchateau, 2008).

Previous studies using IMT have focused only on change in clinical symptoms, such as forced vital capacity and quality of life after period of exercise (Riera et al., 2001). However, no studies have examined the effect of air hole size change on the patient's exercise intensity and the changes in muscle activity of the inspiratory main and accessory muscle during breathing exercise using different

air hole diameter of air tip of the IMT.

2. Purpose of study

The purpose of our study was to investigate the effect of air hole diameter size change of air tip on the rating of perceived exertion and muscle activity of the inspiratory primary and accessory muscle during breathing exercise using IMT in healthy young subjects. The hypothesis of this study was as follows: depending on the difference in diameter of air tip of the IMT, the rating of perceived exertion and muscle activity of the inspiratory primary main and accessory muscle would be different during breathing exercise using IMT.

II . Methods

1. Participants

Sample size was determined with software of G*power analysis. Necessary sample size of 14 was calculated through a power of 0.80 and effect size of 0.37 (calculated with a partial η^2 of 0.121 from a pilot study with five subjects) with a α level of 0.05. As a result, fifteen healthy male subjects voluntarily participated in this study (Table 1). Informed consent form was signed by individual subjects after understanding the purposes and methods of this present study. Exclusion criteria were as follows: 1) subjects who complained of pain or discomfort during breathing exercise with IMT, 2) subjects who were diagnosed with musculoskeletal diseases or cardiorespiratory disorders, 3) subjects who have been receiving recent operations or taking any medications affecting breathing patterns. Institutional review board of Hoseo University has approved this study (104123-170904-HR-063-02).

Table 1. Subject demographic characteristics and pulmonary functions

Ethnicity	Sex	Age (y)	Height (cm)	Weight (kg)	BMI (kg/m ²)	FVC (L)
Korean	Male	21.6±1.8	174.87±5.15	69.59±7.91	22.81±2.96	3.4±0.6

BMI; body mass index, FVC; forced vital capacity

2. Measurements

1) Forced vital capacity (FVC)

To measure the forced vital capacity, Desk-top Spirometer (Spirometer, Pony F/X, Italia) was used. In sitting position, the subjects inhaled as deep as possible and then exhaled maximally into the spirometer.

2) Borg's perceived exertion scale

To measure the subject's difficulty during strengthening exercise of inspiratory muscles, Borg's perceived exertion scale was used. The Borg's perceived exertion scale consists of 20 score from 6 score and the higher score means the harder perception.

3) Data collection

For surface electromyography (EMG) data collection and analysis, a Noraxon TeleMyo 2400 system (DTS EMG system, Noraxon, Inc, USA) and a Noraxon MyoResearch 1.06 XP software was used. The EMG signals were collected at 1000 Hz amplified, band-pass filtered at 20 and 450 Hz, notch filtered at 60 Hz and processed into the root-mean-square values. EMG data were recorded from the anterior scalene (AS), sternocleidomastoid (SCM), pectoralis major (PM), upper trapezius (UT), external intercostal (EI), and diaphragm (DIA) on the dominant side. After shaving and rubbing the skin with alcohol, disposable Ag/AgCl surface electrodes were attached approximately 2 cm apart and parallel to the each muscle fiber at the frequently referenced site (Chien et al., 2008; Cram, 1998); (1) AS, electrode was placed on the just posterior to and at a

slightly oblique angle relative to the SCM, just above the clavicle and in the hollow triangle anterior to the UT; (2) SCM, electrode was positioned slightly posterior from the middle of the distance between the mastoid process and the sternal notch; (3) PM, electrode was placed on the chest wall at an oblique and angle toward the clavicle, approximately 2 cm inferior from the clavicle, just medial to the axillary fold; (4) UT, electrode was positioned along the ridge of the shoulder, slightly lateral to and one-half the distance between the cervical spine 7 and the acromion; (5) EI, electrode was placed on the second or third intercostal space at the midclavicular line; (6) DIA, electrode was positioned 7th or 8th intercostal space on the dominant side of the body at the midclavicular line. Maximal voluntary isometric contractions (MVIC) were collected to normalize the EMG data from each muscle (AS, SCM, PM, and UT) during 5 seconds. The position of each muscle for MVIC was (1) for AS and SCM, the subject was positioned supine with elbows flexed, hands beside the head, craniocervical and cervical anterolateral flexion; (2) for PM, the subject was positioned sitting on the table with elbow extended and shoulder flexed at 90 °, rotated medially, horizontally adducted toward the sternal end of the clavicle; (3) for UT, the subject positioned sitting on the table with shoulder abducted at 90 ° and cervical ipsilateral flexion and contralateral rotation (McCreary & Provance, 2005). The middle 3-s of MVIC was used for data analysis. The mean value of two trials for each muscle was used for data analysis. The mean EMG amplitude values for SCM, AS, PM, UT were described as a percentage of MVIC (%MVIC) (de Oliveira et al., 2008). The intraclass correlation coefficient of EMG was 0.996 (95 % confidence

interval: 0.989-0.999) in this study.

3. Procedure

First, the subject who visited the laboratory listened to the purpose of the study and the experiment method while sitting comfortably in the chair. Then, primary investigator explained the method of Borg's exertion scale. After the agreement of research participation, the subject took off the top and was attached electrodes on his body.

The subjects were instructed to breath in their normal habitual comfortable breathing style with IMT (Inspiratory

muscle trainer, Smiths Medical ASD. Inc, USA) in sitting position with 90 ° of hip, knee and ankle. The order of three difference air hole diameter of the air tips (yellow color for 6 mm, blue color for 4 mm, and red color for 2 mm) for IMT was randomized using the random number generator in Microsoft Excel (Excel, Microsoft Corp., USA) (Fig 1). After subjects adapted to breathe using IMT, subjects performed breathing exercise with IMT for 1 minute for the data collection. All EMG data during breathing exercises with IMT were recorded for 1 minute. The middle 30 seconds were used for data analysis.

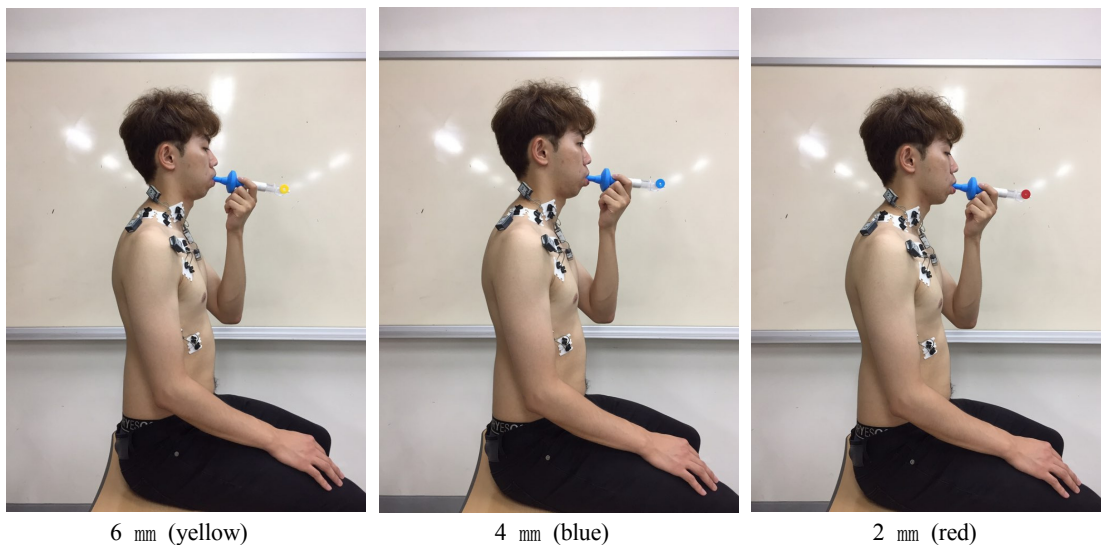


Fig 1. Breathing exercise with different diameter of IMT

4. Statistical analysis

SPSS version 25.0 (SPSS, IBM Inc, USA) was used for test the differences between conditions. After the results are changed as logit because of normal distribution, one way analysis of variance with repeated measured was employed for comparison for three difference diameters (yellow color, blue color, and red color) for IMT. In the case of significant differences between test positions, Bonferroni's post hoc test was performed. In all analyses, p-values <0.05

were deemed to indicate statistical significance.

III. Results

The muscle activities of the AS (F=4.535b, P=0.032), SCM (F=4.482b, p=0.033), UT (F=4.736b, p=0.029), and RPE (F=147.072b, p=0.001) are increased significantly in accord to decreasing diameter of air hole of air tip in IMT. There are no differences in muscle activities of the PM

($F=0.157b$, $p=0.856$), EI ($F=0.342b$, $p=0.717$), DIA ($F=1.249b$, $p=0.319$) in accord to differences of diameter of air hole of air tip in IMT. In Bonferroni's post-hoc test, there are significant differences between 6 mm and 2 mm ($p=0.007$), and between 4 mm and 2 mm ($p=0.016$) in AS,

between 6 mm and 2 mm ($p=0.014$) in SCM, and between 6 mm and 2 mm in UT ($p=0.016$), and between all matching of 6 mm and 4 mm ($p=0.001$), 6 mm and 2 mm ($p=0.001$), and 4 mm and 2 mm ($p=0.002$) in RPE (Table 2).

Table 2. Logit comparisons among 3 different diameters of IMT (Mean \pm standard deviation)

	6 mm (yellow)	4 mm (blue)	2 mm (red)	F	p
AS	1.161 \pm 0.696	1.249 \pm 0.701	1.622 \pm 0.854 ^{† †}	4.535	0.032
SCM	-.035 \pm 0.665	0.047 \pm 0.639	0.347 \pm 0.852 [†]	4.482	0.033
PM	-.104 \pm 0.889	-.115 \pm 0.867	-.167 \pm 0.741	0.157	0.856
UT	-.250 \pm 0.903	-.044 \pm 1.221	.193 \pm 1.144 [†]	4.736	0.029
EI	1.475 \pm 0.478	1.535 \pm 0.475	1.417 \pm 0.230	0.451	0.642
DIA	2.031 \pm 0.651	1.964 \pm 0.725	2.139 \pm 0.681	1.228	0.308
RPE	1.9164 \pm 0.265	2.193 \pm 0.265 [†]	2.779 \pm 0.109 ^{† †}	98.712	0.000

*significant differences among three diameters of IMT air-hole ($p<0.05$)

Post-hoc: [†] significant difference to 6 mm ($p<0.017$), ^{††} significant difference to 4 mm ($p<0.017$)

AS; anterior scalene, SCM; sternocleidomastoid, PM; pectoralis major, UT; upper trapezius, EI; external intercostal, DIA; diaphragm, RPE; rating perceived exertion

IV. Discussion

The hypothesis of this study was that depending on the difference in diameter of the IMT air tip, the RPE and muscle activity of the inspiratory principal (DAI and EI) and inspiratory accessory muscle (AS, SCM, PM and UT) would be different during breathing exercise using IMT. There were significant differences among the parameters in muscle activities of the AS, SCM, and UT and RPE. Hence, our research hypothesis was partially supported.

As decreasing of air hole diameter of tip in IMT, the several muscle activities of the inspiratory accessory muscles (AS, SCM, and UT) were increasing significantly. Previous results also showed significantly increased SCM activity during loading periods using IMT in chronic obstructive pulmonary disease (De Andrade et al., 2005). These results could be caused by increasing resistance of

air flow (caused by decreasing of air hole diameter of tip in IMT) during inspiratory breathing phase (Dodd et al., 1984). The resistance of air flow increases muscular efforts to elevate upper chest wall and to obtain the amount of tidal volume in upper airway during inspiration.

There was no significant differences in muscle activities of the inspiratory accessory muscle (PM). This result was caused by no distal fixation of arm and no mechanical advantage (block the role as an arm mover, and devote itself on trunk elevator) for the PM as an inspiratory accessory muscle (Vera-Garcia et al., 2010). Also there were no significant differences in muscle activities of the inspiratory primary muscles (EI and DIA) in accordance to decreasing of air hole diameter of tip in IMT. These results were caused by compensatory function of inspiratory accessory muscles (AS, SCM, and UT) to overcome the increasing resistance for primary muscles during inspiratory

phase, and might be caused by that resistance of mouth piece (through air hole of air tip in IMT) affect only the movement of upper chest wall (Corrêa & Bérzin, 2008). However, the results of muscles (EI and DIA) could be investigated with further objective research, because our research did not adapt the %MVIC for the EI and DIA with comparable other muscles (AS, SCM, PM and UT).

As decreasing of air hole diameter of tip in IMT, RPE was increasing significantly. These result were caused by same reason of the muscle activities in inspiratory accessory muscles (AS, SCM, and UT). The breathing exercises for strengthening inspiratory muscles often cause pain of trunk muscles and dyspnea. These features might be caused by fatigable condition of the inspiratory accessory muscles (HajGhanbari et al., 2012). Hence, RPE could be an objective target point to prevent fatigue of inspiratory accessory muscles and respiratory burden. Moderate intensity of strengthening exercise with inspiratory muscle trainer might elicit favorable change in patients' condition without unwanted effects (Romer et al., 2002).

There were several limitations in our research. The first, adapted sitting posture in this study is not favorable deep breathing posture after increasing ventilator demand condition. In previous studies, trunk leaning forward posture with arm support could be a recommendable posture to improve the function of inspiratory accessory muscles. As these mechanical advantages, chronic respiratory patients select trunk leaning forward posture with arm support for the relaxation and athletic players make these pose after running competition for resolution the hyper ventilator condition. Hence, several recommendable posture could be adapted for further research. The second, surface EMG could not be a suitable device to collect the EMG data of DIA. Previous studies have described this limitation in their research, therefore the data of DIA would be contaminated with artifact or not. Hence, further advanced design to collect EMG data of DIA would be adapted for the explanation of core muscular function.

V. Conclusion

The decreasing the diameter of air-hole induces increasing muscle activities of the inspiratory accessory muscles. The exercise intensity for the chronic patients with dyspnea should be lower than patients without dyspnea. Even with same condition of exercise intensity, the all-day using inspiratory muscles of chronic patients with dyspnea, could be faster fatigable than patients without dyspnea. The exercise intensity for the chronic patients with dyspnea should be adjusted to their cardiopulmonary symptoms at initial evaluation.

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