# Facilitated Protein-DNA Binding: Theory and Monte Carlo Simulation ${ }^{\dagger}$ 

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#### Abstract

The facilitated diffusion effect on protein-DNA binding is studied. A rigorous theoretical approach is presented to deal with the coupling between one-dimensional and three-dimensional diffusive motions. For a simplified model, the present approach can provide numerically exact results, which are confirmed by the lattice-based Monte Carlo simulations.


Key Words: Diffusion-influenced reaction, Facilitated diffusion, Protein-DNA binding, Dimension reduction, Exact solution

## Introduction

One of central questions in molecular biology is how a DNA-binding protein searches for a specific binding site on DNA. The protein can find its target much faster than simple diffusion-reaction theories predict. Numerous experimental and theoretical studies ${ }^{1-19}$ make us believe that diffusive sliding along DNA greatly facilitates the binding process between DNA and protein.
From the viewpoint of diffusion-influenced reaction theories, the facilitated diffusion problem has two coupled mechanisms of the three-dimensional (3D) nonspecific binding to a random site on DNA and the one-dimensional (1D) sliding along DNA to the specific binding site, as illustrated in Figure 1. Even if each mechanism can be solved analytically, the coupling between the two prohibits us from obtaining the exact analytical results. Most previous theoretical approaches treated the diffusion-reaction process on the basis of the phenomenological rate law. In this paper, a rigorous theoretical approach is presented to provide numerically exact solutions for a simplified model of the facilitated diffusion-reaction problem. The lattice-based Monte Carlo simulations are also performed to confirm our theoretical predictions.

## Theory

As an archetype of the facilitated diffusion-influenced reaction between a protein and a specific binding site on DNA, we assume the DNA-binding protein as a sphere and the DNA strand as an infinite cylinder. When the protein encounters the DNA within the distance $R_{r}$ by diffusion in the bulk cytoplasm, the protein is assumed to be trapped on the DNA strand. Without loss of generality, we can regard the protein as a point particle and the DNA as a cylinder with radius $R_{r}$ along z-axis. The specific binding site is

[^0]modeled with a reactive cylinder in DNA located at origin. The trapped protein searches for the binding site by 1D sliding. The search ends when the protein encounters the reactive cylinder within the distance $R_{z}$. The simplified model is illustrated in Figure 1. The reaction can occur in two ways. One is the direct encounter with the reactive cylinder by diffusion in 3D and the other is the two-step reaction by coupling of 1D and 3D diffusive motions.

Let us denote the probability density to find a free protein at time $t$ as $p(r, z, t)$ in cylindrical coordinates $r$ and $z$. Similarly, $p\left(*_{r}, z, t\right)$ is the probability density for a protein trapped on the DNA strand and $p\left(*_{r}, *_{z}, t\right)$ is the specific binding reaction probability. Here, $*_{r}$ denotes the trapped state and $*_{z}$ denotes the bound state. Then, the evolution of reaction-diffusion equations are as follows:

$$
\begin{equation*}
\frac{\partial p(r, z, t)}{\partial t}=\mathcal{L}_{\text {free }} p(r, z, t) \tag{1}
\end{equation*}
$$



Figure 1. Schematic representation of protein-DNA binding by the facilitated diffusion. In the left figure, the searching process consists of 3D and 1D diffusive motions. In the right figure, our simplified model is presented. The protein is regarded as a point particle, DNA is an infinite cylinder along z-axis, and the specific binding site is a color cylinder at origin in the cylindrical coordinate.

$$
\begin{equation*}
\frac{\partial p\left(*_{r}, z, t\right)}{\partial t}=H\left(|z|-R_{z}\right) \mathcal{L}_{\text {trap }} p\left(*_{r}, z, t\right), \tag{2}
\end{equation*}
$$

where $r \geq R_{r},-\infty<z<\infty$, and $H(z)$ is the Heaviside step function. The diffusion operators without an interaction potential are defined as

$$
\begin{gather*}
\mathcal{L}_{\text {free }}=D_{r}\left(\frac{\partial^{2}}{\partial r^{2}}+\frac{1}{r} \frac{\partial}{\partial r}\right)+D_{z} \frac{\partial^{2}}{\partial z^{2}},  \tag{3}\\
\mathcal{L}_{\text {trap }} \equiv D_{\text {trap }} \frac{\partial^{2}}{\partial z^{2}} \tag{4}
\end{gather*}
$$

with the corresponding mutual diffusion constants $D_{r}, D_{z}$, and $D_{\text {trap }}$.

To make the problem tractable, here, we consider only the perfect irreversible trapping and binding, which means that every encounter leads to the trapping and binding and reversible untrapping and unbinding are not allowed. Then, for an initially free state, namely,

$$
\begin{equation*}
p\left(r, z, 0 \mid r_{0}, z_{0}\right)=\frac{\delta\left(r-r_{0}\right) \delta\left(z-z_{0}\right)}{2 \pi r} \tag{5}
\end{equation*}
$$

we can solve Eq. (1) by using separation of variables and obtain the Green function as a product solution ${ }^{20}$ of wellknown functions,

$$
\begin{equation*}
p\left(r, z, t \mid r_{0}, z_{0}\right)=p_{r}\left(r, t \mid r_{0}\right) G_{z}\left(z, t \mid z_{0}\right) \tag{6}
\end{equation*}
$$

where $G_{z}\left(z, t \mid z_{0}\right)$ is the 1D Green function of a free particle ${ }^{21}$

$$
\begin{equation*}
G_{z}\left(z, t \mid z_{0}\right)=\frac{1}{\sqrt{4 \pi D_{z} t}} \exp \left[-\frac{\left(z-z_{0}\right)^{2}}{4 D_{z} t}\right] \tag{7}
\end{equation*}
$$

and the two-dimensional (2D) function $p_{r}\left(r, t \mid r_{0}\right)$ can be obtained in the Laplace-transformed $\left[f(s)=\int_{0}^{\infty} f(\tau) e^{-s \tau} d \tau\right]$ domain as ${ }^{21}$
$\tilde{p}_{r}\left(r, s \mid r_{0}\right)=\frac{K_{0}\left(\zeta^{\max } \sqrt{s \tau_{r}}\right)}{k_{D_{r}} K_{0}\left(\sqrt{s \tau_{r}}\right)}\left[K_{0}\left(\sqrt{s \tau_{r}}\right) I_{0}\left(\zeta^{\min } \sqrt{s \tau_{r}}\right)-I_{0}\left(\sqrt{s \tau_{r}}\right) K_{0}\left(\zeta^{\min } \sqrt{s \tau_{r}}\right)\right]$.
Here, $\zeta^{\text {max }}=\max \left(r, r_{0}\right) / R_{r}$ and $\zeta^{\min }=\min \left(r, r_{0}\right) / R_{r}$ and the diffusion control rate constant and time scale are defined as $k_{D_{r}}=2 \pi D_{r}$ and $\tau_{r} \equiv R_{r}^{2} / D_{r}$, respectively. $K_{n}(x)$ and $I_{n}(x)$ are the modified Bessel functions of order $n$. Integrating Eq. (8) gives the survival probability

$$
\begin{equation*}
\tilde{S}_{r}\left(s \mid r_{0}\right) \equiv \int_{R_{r}}^{\infty} 2 \pi r d r \tilde{p}_{r}\left(r, s \mid r_{0}\right)=\frac{1}{s}\left[1-\frac{K_{0}\left(\sqrt{s \tau_{r}} r_{0} / R_{r}\right)}{K_{0}\left(\sqrt{s \tau_{r}}\right)}\right] . \tag{9}
\end{equation*}
$$

We can use well-known numerical inverse Laplace-transform algorithms ${ }^{22}$ for Eqs. (8) and (9).

The solution for an initially trapped state at $z_{0}$ is also wellknown as

$$
\begin{align*}
& p\left(*_{r}, z, t \mid *_{r}, z_{0}\right)=\frac{H\left(\left|z_{0}\right|-R_{z}\right) H\left(|z|-R_{z}\right)}{\sqrt{4 \pi D_{\text {trap }} t}} \times \\
& \quad\left\{\exp \left[-\frac{\left(z-z_{0}\right)^{2}}{4 D_{\text {trap }} t}\right]-\exp \left[-\frac{\left(\left|z+z_{0}\right|-2 R_{z}\right)^{2}}{4 D_{\text {trap }} t}\right]\right\}, \tag{10}
\end{align*}
$$

and integrating Eq. (10) over $z$ leads to

$$
\begin{equation*}
S_{\text {trap }}\left(t \mid *_{r}, z_{0}\right)=H\left(\left|z_{0}\right|-R_{z}\right)\left[1-\operatorname{erfc}\left(\frac{\left|z_{0}\right|-R_{z}}{\sqrt{4 D_{\text {trap }} t}}\right)\right] \tag{11}
\end{equation*}
$$

where $\operatorname{erfc}(x)$ is the complementary error function.
Now, we suppose that a free diffusing particle is trapped on the nonspecific position $z^{\prime}$ at time $t^{\prime}$ and slides until time $t$. Then, the probability density function of the particle is proportional to $k_{r}\left(t^{\prime} \mid r_{0}\right) G_{z}\left(z^{\prime}, t^{\prime} \mid z_{0}\right) p\left(*_{r}, z, t-t^{\prime} \mid *_{r}, z^{\prime}\right)$, where the time-dependent trapping rate is defined as

$$
\begin{equation*}
k_{r}\left(t \mid r_{0}\right) \equiv-\frac{d S_{r}\left(t \mid r_{0}\right)}{d t}=\left.k_{D_{r}} R_{r} \frac{\partial p_{r}\left(r, t \mid r_{0}\right)}{\partial r}\right|_{r=R_{r}} . \tag{12}
\end{equation*}
$$

Since $z z^{\prime}>0$ for the irreversible trapping and specific binding reactions, we have

$$
\begin{align*}
& p\left(*_{r}, z, t \mid r_{0}, z_{0}\right)=\int_{0}^{t} d t^{\prime} k_{r}\left(t^{\prime} \mid r_{0}\right) \\
& \times \int_{-\infty}^{\infty} d z^{\prime} H\left(\left|z^{\prime}\right|-R_{z}\right) H\left(z z^{\prime}\right) G_{z}\left(z^{\prime}, t^{\prime} \mid z_{0}\right) p\left(*_{r}, z, t-t^{\prime} \mid *_{r}, z^{\prime}\right) . \tag{13}
\end{align*}
$$

When $z_{0}=0$, this equation, by symmetry, reduces to

$$
\begin{equation*}
p\left(*_{r}, z, t \mid r_{0}, 0\right)=2 \int_{R_{z}}^{\infty} \int_{0}^{t} d z^{\prime} d t^{\prime} k_{r}\left(\tau \mid r_{0}\right) G_{z}\left(z^{\prime}, t^{\prime} \mid 0\right) p\left(*_{r}, z, t-t^{\prime} \mid *_{r}, z^{\prime}\right) . \tag{14}
\end{equation*}
$$

The total survival probability function without the specific binding can be obtained as

$$
\begin{equation*}
S\left(t \mid r_{0}, z_{0}\right)=S_{\text {free }}\left(t \mid r_{0}, z_{0}\right)+S_{\text {trap }}\left(t \mid r_{0}, z_{0}\right) \tag{15}
\end{equation*}
$$

where

$$
\begin{align*}
& S_{\text {free }}\left(t \mid r_{0}, z_{0}\right)=\int_{R_{r}}^{\infty} \int_{-\infty}^{\infty} d z d r 2 \pi r p\left(r, z, t \mid r_{0}, z_{0}\right)=S_{r}\left(t \mid r_{0}\right)  \tag{16}\\
& S_{\text {trap }}\left(t \mid r_{0}, z_{0}\right)=\int_{-\infty}^{\infty} d z p\left(*_{r}, z, t \mid r_{0}, z_{0}\right) \\
& \quad=\int_{0}^{t} d t^{\prime} k_{r}\left(t^{\prime} \mid r_{0}\right) \int_{R_{z}}^{\infty} d z^{\prime}\left[G_{z}\left(z^{\prime}, t^{\prime} \mid z_{0}\right)+G_{z}\left(-z^{\prime}, t^{\prime} \mid z_{0}\right)\right] S_{\text {trap }}\left(t-t^{\prime} \mid *_{r}, z^{\prime}\right) \tag{17}
\end{align*}
$$

Note that these equations are formally exact. However, since $S_{r}\left(t \mid r_{0}\right)$ and therefore $k_{r}\left(t \mid r_{0}\right)$ are known only in the Laplacetransformed domain, we cannot obtain the closed-form expression of $S\left(t \mid r_{0}, z_{0}\right)$. By integrating Eq. (17) numerically, we can obtain the numerically exact results. For the numerical integration of Eq. (17), the following recent approximation for $S_{r}\left(t \mid r_{0}\right)$ in the time domain, which was reported to be accurate for all times, ${ }^{23}$ may be useful:

$$
\begin{equation*}
S_{r}\left(t \mid r_{0}\right) \cong \min \left[1-\sqrt{\frac{R_{r}}{r_{0}}} \operatorname{erfc}\left(\frac{r_{0}-R_{r}}{2 \sqrt{D_{r} t}}\right), \frac{\ln \left(r_{0} / R_{r}\right)}{\ln \left(\sqrt{\pi t /} \tau_{r}+1\right)}\right] \tag{18}
\end{equation*}
$$

Normalization conditions are given by

$$
\begin{gather*}
S_{\text {free }}\left(t \mid r_{0}, z_{0}\right)+S_{\text {trap }}\left(t \mid r_{0}, z_{0}\right)+p\left(*_{r}, *_{z}, t \mid r_{0}, z_{0}\right)=1  \tag{19}\\
S_{\text {trap }}\left(t \mid *_{r}, z_{0}\right)+p\left(*_{r}, *_{z}, t \mid *_{r}, z_{0}\right)=1 \tag{20}
\end{gather*}
$$

Inserting Eq. (11) into Eq. (20), we have

$$
\begin{equation*}
p\left(*_{r}, *_{z}, t \mid *_{r}, z_{0}\right)=H\left(\left|z_{0}\right|-R_{z}\right) \operatorname{erfc}\left(\frac{\left|z_{0}\right|-R_{z}}{\sqrt{4 D_{\text {trap }} t}}\right)+H\left(R_{z}-\left|z_{0}\right|\right) . \tag{21}
\end{equation*}
$$

## Results and Discussions

To confirm our theoretical predictions, we perform lattice-


Figure 2. The time-dependent survival probability of a protein. Simulation results (open circles) are compared with those (solid lines) of Eq. (15) for two different initial conditions: at $x_{0}=y_{0}=z_{0}$ (blue) and on the xy-plane (red).
based Monte Carlo simulations for the present model system. ${ }^{24}$ An initially implanted particle moves by random walk in 3D lattice. When the particle reaches the cylindrical trap, the trapping occurs if $|z|>R_{z}$ or the binding reaction with the reactive cylinder occurs if $|z| \leq R_{z}$. Once trapped particle diffuses along the cylinder until the binding reaction occurs. The lattice constant should be small enough to reproduce the known theoretical results. All simulations are done for more than $10^{8}$ time-steps $\left(t \sim 10^{3}\right)$ and at least $10^{5}$ independent trajectories are averaged.
Since survival probabilities depend on the initial position, we select two distinct initial positions with the same $\sqrt{r_{0}^{2}+z_{0}^{2}}=1.5$ : at $x_{0}=y_{0}=z_{0}\left(r_{0}=1.22\right.$ and $\left.z_{0}=0.87\right)$ and on the xy-plane ( $r_{0}=1.5$ and $z_{0}=0$ ). In both cases, diffusion constants are the same $\left(D_{r}=D_{z}=D_{\text {trap }}=1\right)$ and $R_{r}=R_{z}=1$. In Figure 2, simulation results for $S\left(t \mid r_{0}, z_{0}\right)$ are compared with numerical solutions of Eqs. (15)-(17). One can see that two results are nearly identical. We believe that the small deviations at long times come from the numerical integration of Eq. (17). As expected, the survival probability decreases more rapidly when the initial position is closer to the cylindrical trap.

To study effects of the facilitated diffusion, we compare the theoretical predictions of above two cases with other data in Figure 3. First, simulation results without the cylindrical trap are compared since no analytical result is known. The difference shows the facilitated diffusion effects. The biggest difference is the existence of an escape probability. When the dimensionality is larger than 2 , there is always an escape probability, which is realized by the plateau region in the figure. Adding an infinite cylindrical trap to the system, the dimensionality effectively reduces to 2 and the protein always reaches the DNA strand and eventually the specific binding site at long times. Therefore, the ratio of the reaction rate in the normal diffusion case to that in the facilitated diffusion case goes up to infinity in the macroscopic time limit.


Figure 3. The time-dependent survival probability of a protein for two initial conditions: (a) $x_{0}=y_{0}=z_{0}$ (b) $z_{0}=0$. The blue and red solid lines are the same as those in Figure 2. The black solid lines are obtained from the simulation without an infinite cylindrical trap. The dashed lines are obtained numerically from Eq. (16).

For comparison, we also plot $S_{r}\left(t \mid r_{0}\right)$ or $S_{\text {free }}\left(t \mid r_{0}, z_{0}\right)$, which can be evaluated from Eq. (9) or from simulation results. We confirm that the simulation results reproduce Eq. (9). At short times, the results of $S\left(t \mid r_{0}, z_{0}\right)$ seems similar to those of $S_{r}\left(t \mid r_{0}\right)$. In the intermediate time region, the difference between $S\left(t \mid r_{0}, z_{0}\right)$ and $S_{r}\left(t \mid r_{0}\right)$, namely, $S_{\text {trap }}\left(t \mid r_{0}, z_{0}\right)$ becomes larger. In the long time limit, $S\left(t \mid r_{0}, z_{0}\right)$ apparently converges to $S_{r}\left(t \mid r_{0}\right)$ again. Therefore, $S\left(t \mid r_{0}, z_{0}\right)$ strongly depends on $S_{r}\left(t \mid r_{0}\right)$, in other words, the specific binding rate strongly depends on the nonspecific binding rate. This can be understood by the fact that the 1 D searching rate of the trapped protein is much faster than the 2D trapping rate.

## Conclusion

We have presented a rigorous theoretical approach for the celebrated facilitated diffusion problem. The theoretical method can provide numerically exact results for a simplified model by solving the coupling effect between one- and three-dimensional diffusive motions. The theoretical results are confirmed by the lattice-based Monte Carlo simulations.

The rate enhancement by the facilitated diffusion results from the dimensionality reduction. The three-dimensional diffusive motion reduces to two-dimensional plus one-dimensional motions. The escape probability in three dimensions goes to zero in the reduced dimensions. Therefore, the ratio of the reaction rate in the normal diffusion case to that in the facilitated diffusion case goes up to infinity in the macroscopic time scale. Even when the one-dimensional diffusion is much slower than three-dimensional diffusion, ${ }^{17}$ the facilitated effect will appear in a different time region.
In reality, the cell environment is much more complicated. The cytoplasm is crowded and one-dimensional diffusion along the DNA strand suffers from obstacles and different short-range interactions. However, the key feature of the dimensionality reduction should not vanish. Diffusion usually results from many kinds of collisions in the presence of obstacles and if one-dimensional and three-dimensional "diffusions" can be assumed to include complicated effects, our theoretical predictions should be useful.
More thorough studies may include effects of the finite reactivity, the finite cylinder size, and so forth. Other kinds of dimensionality reductions can be studied in a similar way. Since more complicated two-dimensional diffusion-influenced reactions were reported, ${ }^{25,26}$ these results can be applied to the present problem dealing with different mechanisms. These will be reported elsewhere.

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