

Liposome/Tat Complex for Facilitating Genistein Uptake into B16 Melanoma Cells

Young Mi Park, MyungJoo Kang, Ki Young Moon, Sang Han Park,
Mean Hyung Kang and Young Wook Choi[†]

Division of Pharmaceutical Science, College of Pharmacy, Chung-Ang University,
221 Heuksuk-dong, Dongjak-gu, Seoul 156-756, Korea

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ABSTRACT – Genistein (GT), a major isoflavone found in soybeans, has a potent antioxidant effect that protects the skin from UV-induced damages and malignant melanoma. In order to enhance the cellular uptake of GT, liposome/Tat complexes were prepared by an electrostatic interaction of anionic liposome (DMPC/DCP, 9:1 in molar ratio) with Tat peptide (0.02 to 0.08 mole), one of the well-known cell penetrating peptide (CPP). As the amount of Tat increased, the size increased but the zeta potential decreased. In vitro release study with dialysis membrane elicited GT release from liposomal preparations in a controlled manner. The addition of Tat increased GT release, especially for the initial period. In the cellular uptake study by incubating B16 melanoma cells with various liposomal preparations containing GT, B16 melanoma cells demonstrated a time-dependent increase of drug accumulation. Compared to the aqueous GT suspension, intracellular uptake was substantially enhanced by anionic liposomal formulation and further increased by the complex formulation. Therefore, liposome/Tat complex might be a good candidate for facilitating intracellular drug delivery.

Key words – Genistein, Liposome/Tat complex, B16 melanoma cell, Drug release, Cellular uptake

Among the various cancers cells, human melanoma cells are well-known to have less antioxidant capacity than that of normal melanocytes. Moreover, melanoma cells are capable of producing large amounts of superoxide anions without stimulants, which are implicated in metastasis by promoting endothelial injury (Ichihashi et al., 2000; Wei et al., 2003; Sander et al., 2004). Genistein (GT), one of the major isoflavones in Leguminosae, has been attractive because epidemiologic studies showed that consumption of soybean-containing diets was associated with a lower incidence of certain human cancers in Asian populations (Barnes et al., 1990). Such chemopreventive and antineoplastic effects of GT were related with the antioxidant activity and inhibitory activities on cell proliferation and angiogenesis (Spinozzi et al., 1994; Zhou et al., 1998; Booth et al., 1999; Vedavanam et al., 1999; Surh et al., 2001). However, due to poor solubility and poor permeability of GT, clinical applications are very limited (Rimbach et al., 2003; Motlekar et al., 2006). Oral bioavailability of GT has been extensively studied (Kwon et al., 2007).

One approach to circumvent the problem of low efficiency of cellular uptake is to incorporate peptides that are capable of penetrating the plasma membrane. Such peptides, called protein transduction domains (PTD) or cell-penetrating peptides

(CPP), are either derived from naturally occurring proteins or artificially designed peptides. A number of CPP have been successfully used to deliver drugs, protein and even DNA into cells (Hyndman et al., 2004). One of the shortest peptides containing a nuclear localization signal (NLS), Tat 48-60, was defined as the minimal translocating fragment (Temsamani and Vidal, 2004). These Tat peptides derived from the HIV type 1 Tat protein facilitate intracellular delivery of macromolecules and small colloidal particles.

Another way for increasing the delivery of drugs is the use of vesicular systems such as liposomes (Kang et al., 2010). Due to their biocompatibility and the capability of incorporating both hydrophilic and lipophilic drugs, liposomes are widely used as delivery systems for a broad spectrum of agents including chemotherapeutics, imaging agents, antigens, lipids and DNA (Martyet al., 2004). Moreover, therapeutic molecules are protected by the lipid bilayer of the liposome from metabolism and enzymatic degradation. It was also demonstrated that relatively large drug carriers, such as 200nm liposomes, can also be delivered into cells by Tat peptide attachment to the liposome surface (Torchilin et al., 2001).

Therefore, in the present study, liposome/Tat complexes have been developed for facilitating GT delivery into B16 melanoma cells. Along with physical characterization of the complexes, pharmaceutical evaluations for dispersion stability, in vitro drug release, and cellular uptake efficiency were performed.

[†]Corresponding Author :

Tel : +82-2-820-5609, E-mail : ywchoi@cau.ac.kr
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Materials and Methods

Cell lines and cell culture

The B16 melanoma cells were cultured in Dulbecco's modified Eagle's medium containing 20 mM HEPES/NaOH (pH 7.4), 5 mM NaHCO₃, 10% fetal bovine serum (FBS) and antibiotics (100 µg/mL streptomycin, 100 U/mL penicillin) at 37°C under a humidified condition of 95% air and 5% CO₂.

Chemicals and reagents

Genistein (GT) was provided from Rexgene Biotech Co. (Seoul, Korea). Dimyristoylphosphatidylcholine (DMPC), dicalcium phosphate (DCP), stearylamine (SA), trypsin-EDTA, and N,N-diethylnicotinamide (DENA) were purchased from Sigma Chemical Co. (St. Louis, MO, USA). Synthetic Tat peptide (Arg-Lys-Lys-Arg-Arg-Gln-Arg-Arg-Arg, 9mer) was purchased from Pepton Co. (Taejun, Korea). All other chemicals and reagents purchased from commercial sources were of analytical grade. Double distilled water was used for all experiments.

Preparation of liposomes and liposome/Tat complexes

Liposomes were prepared by conventional film hydration and extrusion method. Briefly, in case of a neutral liposome, DMPC was dissolved in chloroform and methanol mixture (3:2 v/v) along with 30 µM of GT in a round bottom flask. DCP and SA were added to DMPC liposome in 9:1 molar ratio for preparing anionic and cationic liposomes, respectively. Solvent was removed by rotary vacuum evaporation above the lipid transition temperature (Rotary Evaporator, Super fit, Ambala, India) for approximately 30 min, and solvent traces were removed by maintaining the lipid film under vacuum overnight at room temperature. Thin lipid films were then hydrated with double-distilled water by rotation (100 rpm, 40°C, 10 min) and extruded ten times through sandwiches of 200 nm polycarbonate membrane filter (Millipore, USA) to obtain small unilamellar vesicles (SUVs). The final lipid concentrations in all vesicular formulations were approximately 14 mM.

Formation of liposome/Tat complexes was carried out in aqueous dispersion at room temperature. Different amount of Tat was added to anionic liposomes and allowed to stand for 5 min for electrostatic complexation. The molar ratio of DMPC:DCP:Tat were 9:1:0.02 (Complex 1), 9:1:0.04 (Complex 2), and 9:1:0.08 (Complex 3). Complex 2 and complex 3 were re-extruded ten times through 400 nm polycarbonate membrane filters (Millipore, USA), unlikely to complex 1 in which the vesicular size was not changed significantly com-

pared to that of anionic liposome.

Measurement of vesicle size and zeta potential

Physical characteristics of liposomes and liposome/Tat complexes including particle size and size distribution, polydispersity index, and zeta potential were determined by dynamic light scattering (DLS) method with Zetasizer Nano-ZS (Malvern Instrument, Worcestershire, UK). Liposomes and liposome/Tat complexes were diluted 10-fold with double-distilled water for the measurement in triplicates. The stability of liposome and liposome/Tat complexes was determined by comparing the particle size change over time.

Determination of entrapment capacity

The encapsulation efficiency was determined by ultracentrifugation method. Immediately after preparing liposomes and liposome/Tat complexes, the product was ultracentrifuged (48,000g, 4°C, 30 min) to separate the unincorporated drug. After ultracentrifugation, GT content in supernatant and pellet were assayed by HPLC. The entrapment capacity of liposomes and liposome/Tat complexes were calculated as follows: $(T-C)/T \times 100$, where T is the total amount of drug in both the supernatant and pellet, and C is the amount of drug in the supernatant.

In vitro release test

Release of GT from various liposomal formulations was determined at 37°C using Franz diffusion cell mounted with a dialysis membrane (MWCO 12 kDa). Phosphate buffer solution (pH 7.4) containing DENA (1 M) was used as a receptor medium for sink condition. GT solution in 10% DMSO, liposomal suspension, liposome/Tat complexes, and aqueous GT suspension were loaded to donor compartment. At predetermined time points, an aliquot (500 µL) of receptor solution was withdrawn and assayed for GT by HPLC analysis.

Cellular uptake of GT

B16 melanoma cells were seeded at the density of 1×10^5 /well to 6-well dish. After 12 hr, the cells were incubated with GT suspension, liposomal suspension, liposome/Tat complexes. The incubation was stopped by washing the cells with ice-cold PBS (Wang et al., 2005). The cells were harvested by 1x trypsin-EDTA solution and collected by centrifugation at 20,000 g for 5 min. The supernatants were removed and resulting pellets were re-suspended in 1.0 mL PBS. Suspended cells were lysed by sonication (3/1 s, 200W, 10 times) and then centrifuged at 20,000 g for 5 min. The supernatants were transferred to test tube and extracted with 5 mL ethyl acetate. The

mixture was vortexed for 30 min and then centrifuged for 15 min at 4000 g. The upper layer was transferred into another test tube and evaporated to dryness with N₂ stream at 35°C. The residue was reconstituted in 150 µL of 50% methanol and vortexed for 3 min. An aliquot (50 µL) of the solution was injected into the HPLC system for GT assay.

GT assay by HPLC

The concentration of GT was determined by HPLC. The HPLC system consisted of a pump (L-2130), an UV detector (L-2400, $\lambda = 262$ nm), a data station (LaChrom Elite, Hitachi, Japan), and a C₁₈ column (15 cm, ShiseidoTM, Japan). The mobile phase comprised acetonitrile/50 mM ammonium formate buffer solution (4:6 v/v) and was delivered at a flow rate of 1 mL/min. The injection volume was 50 µL and the relative retention time was found to be 4.5 min.

Results and Discussion

Characterization of liposomes and liposome/Tat complexes

To investigate the effect of Tat complexation, Tat was added to anionic liposome in various molar ratios from 0.02 to 0.08 versus DCP content. Vesicular size of anionic liposome was greatly increased by the complexation, revealing the linear relationship between the size and Tat content (data not shown). The size of the complex 1 (Tat ratio of 0.02) was kept in similar range to that of anionic liposome. Beyond this ratio, the

vesicles were larger than 2 µm requiring further size reduction. Therefore, complexes 2 and 3 were prepared by re-extrusion through 400 nm polycarbonate membrane filter. As a result, all liposome/Tat complexes were in the range of 210 to 320 nm in average, a little greater than those of neutral or charged liposomes (Table I). Low polydispersity index of less than 0.3 indicates a narrow and homogeneous size distribution of all liposomal formulations.

Surface charge of liposomes can be manipulated by the addition of charged molecules into the bilayer. Anionic liposome was successfully prepared with DMPC and DCP, having a zeta potential of about -45 mV. By the addition of Tat, a positively charged peptide, the potential of the complexes was decreased proportionally to Tat content. This is an evidence for electrostatic interactions between anionic liposome and Tat peptide to form a complex, and Tat is mostly located at the surface of the complexes as depicted in Figure 1. On the other hand, GT was efficiently loaded into liposomes and liposome/Tat complexes, revealing high entrapment capacity of over 80% in all liposomal formulations. Tat complexation of the anionic liposome did not change the entrapment efficiency of the vesicle, suggesting that the bilayer function was maintained intact and the drug was efficiently encapsulated within the vesicle.

Dispersion stability of liposome/Tat complexes

Aqueous dispersion of liposomal vesicles is stabilized by an appropriate zeta potential, an electric repulsion at shear plane of the particle. Therefore, surface charge including zeta poten-

Table I. Physical characteristics of GT-loaded liposomes and liposome/Tat complexes

| Parameters | Liposome | | | Liposome/Tat Complex | | |
|--------------------------|-------------|-------------|-------------|----------------------|-------------|--------------|
| | Neutral | Cationic | Anionic | Complex 1 | Complex 2 | Complex 3 |
| Mean vesicular size (nm) | 159.1 ± 6.1 | 174.6 ± 4.4 | 194.0 ± 3.3 | 212.8 ± 6.9 | 239.3 ± 6.1 | 318.8 ± 20.3 |
| Polydispersity index | 0.13 ± 0.06 | 0.18 ± 0.06 | 0.23 ± 0.04 | 0.19 ± 0.08 | 0.28 ± 0.01 | 0.26 ± 0.03 |
| Zeta potential (mV) | -14.3 ± 0.3 | +47.4 ± 0.6 | -45.4 ± 1.6 | -38.8 ± 2.3 | -27.2 ± 0.8 | -15.9 ± 0.9 |
| Entrapment capacity (%) | 81.4 ± 3.1 | 80.9 ± 1.5 | 81.9 ± 5.5 | 83.8 ± 3.8 | 84.1 ± 2.1 | 82.9 ± 1.0 |

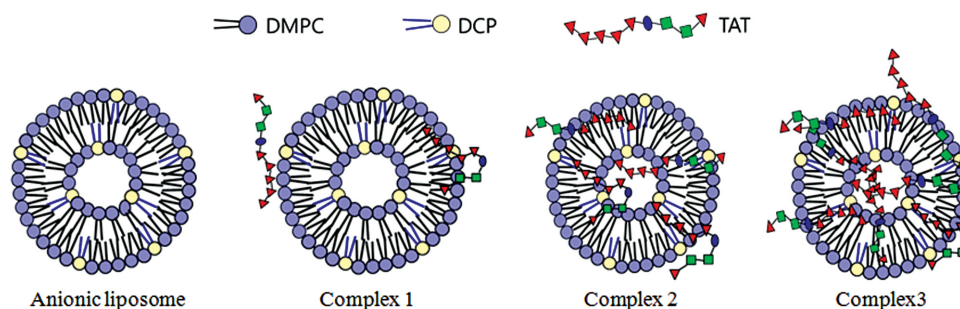


Figure 1. Drawing illustrations of anionic liposome and liposome/Tat complexes.

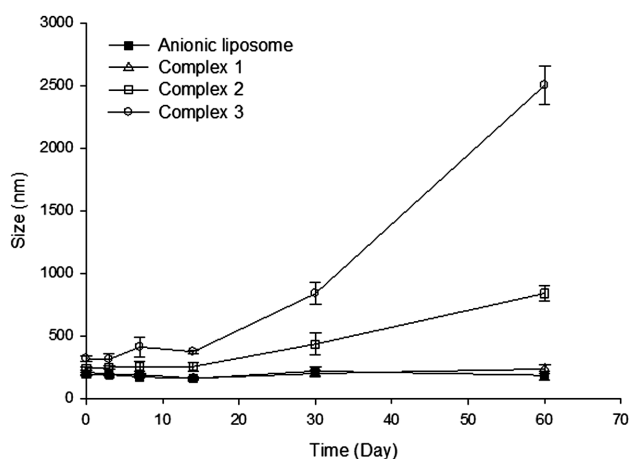


Figure 2. Dispersion stability of liposome and liposome/Tat complexes on storage at 4°C for 60 days.

tial plays a major role for stable dispersion of the vesicles without any aggregation or caking. Physical dispersion stability of anionic liposome and liposome/Tat complexes was determined by the observation of the particle size changes over time. On storage for 60 days at 4°C, as shown in Figure 2, anionic liposome and complex 1 did not show any significant changes in vesicle size. Greater zeta potential (about -40 mV) of both liposomal systems contributed to protect the vesicles from the aggregation of the dispersed phases. Meanwhile, the size of the complexes 2 and 3 was greatly increased upon storage. This might be due to the weaker zeta potential of the complex 2 (-27 mV) and complex 3 (-16 mV), resulting in closer contact of the particles. Therefore, fresh liposomal preparations were further used for the drug release and cellular uptake study, since all liposomal preparations were stable enough for the first two weeks of storage.

In vitro release of GT

To evaluate the drug release property of liposome/Tat complexes, other samples of GT solution in 10% DMSO, liposomal suspension, and aqueous GT suspension were compared (Figure 3). Since the release studies were carried out with a receptor medium offering sink condition for GT, solubilized or unencapsulated drug can be diffused freely through a dialysis membrane. The solubility of GT in water was estimated as 3.04 ng/mL in earlier report (Motlekar et al., 2006). By adding DENA as a hydrotropic agent, GT is very soluble in aqueous receptor medium to provide a sink condition. GT solution brought the fastest release in the earlier stage of release and reached equilibrium afterward. Drug release from aqueous GT suspension was very low, due to its limited solubility in water.

GT was released from liposomal suspension in a controlled

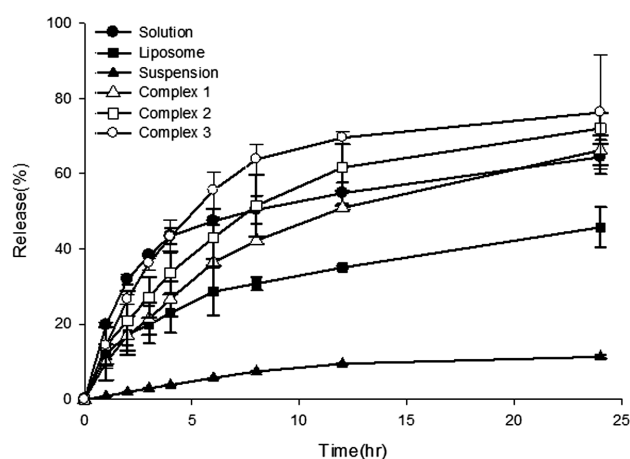


Figure 3. *In vitro* release of GT from various preparations.

manner. The addition of Tat peptide increased GT release, especially for the initial period. As the amount of Tat increased, the release of GT increased as well. Overall order of release was decreased as follows: Complex 3 > Complex 2 > Complex 1 > Anionic liposome. The reason for this phenomenon can be explained by two possibilities. First, Tat addition perturbs the bilayer structure and thereby makes the liposome leaky. Even though the positively-charged peptide binds to the negative charge at the surface, some fragments of Tat peptide sequence could penetrate the liposomal membrane by virtue of its cell penetrating capability in living cells. Secondly, reorientation of Tat peptide may occur, anchoring the hydrophobic domain of the peptide into the bilayer. Complexes 2 and 3 were originally large in vesicle size, and subjected to re-extrusion through 400 nm polycarbonate membrane filter. During this procedure, the bilayer could be re-assembled with a structure of most Tat peptides orienting outwards and some peptides locating at inner compartment or within the lamellae.

Effect of liposome/Tat complex on cellular uptake of GT

Facilitation of cellular uptake was evaluated by incubating B16 melanoma cells with various liposomal preparations containing GT. In the present study, the cold PBS was used to wash cells in order to remove free GT adhering to the cell membranes after incubation. After pretreatment, the values measured by the HPLC assay reflected the amount of GT that was taken up by the B16 melanoma cells. The results for intracellular drug accumulation in B16 melanoma cells after 2, 4 and 6 hr incubation with various preparations including aqueous GT suspension, anionic liposome, and liposome/Tat complexes are shown in Figure 4.

B16 melanoma cells demonstrated a time-dependent increase of drug accumulation in all preparations tested. These results

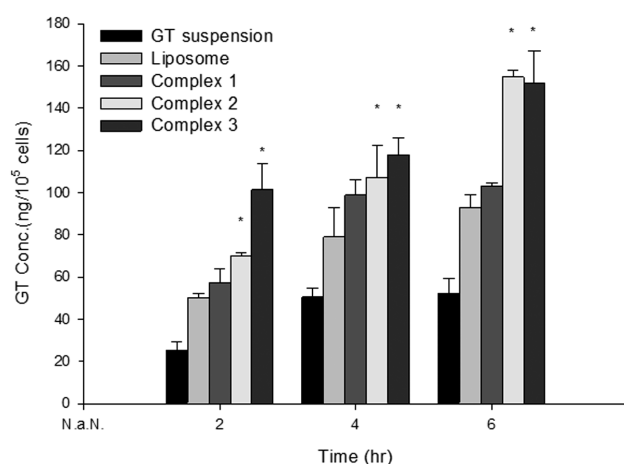


Figure 4. Intracellular drug accumulation in B16 melanoma cells after incubation with various preparations. Results are expressed as the amount of GT/10⁵ cells. Statistical analysis was performed using the Student's t-test (*P<0.05 versus liposome).

indicated that cells exposed to anionic liposome showed more pronounced accumulation than cells exposed to aqueous GT suspension. The intracellular uptake of GT was saturated within 6 hr for the case of GT suspension, because of the low solubility of GT in distilled water. In comparison to GT suspension, intracellular uptake was substantially enhanced by anionic liposomal formulation. It was further increased by liposome/Tat complex formulations. These results are explained by the following reasons. First of all, drug release was greater in liposome/Tat complexes due to their leaky structures. The passive diffusion of GT through the cell membrane could be facilitated. In addition, the encapsulation of drug within CPP-modified liposome resulted in uptake enhancement of drug into cells. Tat peptide originally has the characteristics of penetration effect on cell membranes because of the ability to interact with lipid membranes and to adopt a significant secondary structure (Marty et al., 2004). Therefore, liposome/Tat complex might be a good candidate for facilitating intracellular drug delivery.

Conclusion

In the present study, the effect of Tat peptide complexation with anionic liposome on intracellular delivery of GT was investigated. Liposome/Tat complexes were characterized by physical properties of size distribution, zeta potential, and entrapment capacity. Dispersion stability, in vitro drug release, and cellular uptake efficiency were also evaluated. Finally, we could suggest that the liposome/Tat complex was superior to other conventional liposomes for intracellular delivery of GT.

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