

Quality Assurance in Conformal Radiation Therapy

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Background

The National Cancer Institute has funded several Collaborative Working Groups (CWGs) in the last decade to carry out research projects in the area of 3D treatment planning, beginning with the particle contracts in 1982 and ending with the radiotherapy "Tools" projects, scheduled to complete in March 1994.

In recognition of the state-of-the-art of 3D treatment planning in 1993 the National Cancer Institute is now in the process of funding a Cooperative Group to carry out a clinical trial in 3D conformal radiotherapy.

The headquarters will be located at the offices of the Radiation Therapy Oncology Group (RTOG) in Philadelphia with 3D treatment planning support and quality assurance oversight provided through a subcontract with Washington University at St. Louis.

The task of the Cooperative Group will be to determine a new maximum tolerated dose to the prostate using 3D conformal radiotherapy techniques. Then the Phase I/Phase II dose-searching studies will proceed to Phase III studies, in which patients will be randomized to receive conventional radiotherapy or 3D conformal therapy at the higher dose. The completion of this clinical trial can potentially influence the future of radiotherapy by showing whether 3D radiotherapy techniques have a measurable clinical impact.

The Particle CWG had the most difficult job as they first had to develop the framework of the collaborative group that was to be used by subsequent CWGs. They had to develop such as "mobile" target volume and "immobile" target volume in the concepts of treatment planning. These concepts, initially spawned and developed in the CWGs, although the names have been modified by the International Commission on Radiation Units (ICRU) to be gross tumor volume (GTV), clinical tumor volume (CTV) and planning target volume (PTV). In addition, the Particle CWG developed 1) the first treatment planning protocols for simultaneous tr

reatment planning experiments between institutions using actual patient data, 2) the first formats for exchanging data by magnetic tape, 3) the first models for evaluating competing plans, such as dose-volume- histograms (DVH), tumor control probability(TCP) and normal tissue complication probability(NTCP), and 4) many of the first 3D tools that are now part of every modern 3D treatment planning system.

Volume and Dose Specification for 3D Conformal Radiation Therapy

In ICRU Report 29, the definition of target volume included the oncological safety margin and the planning safety margin. For 3D CRT, a clear separation between these two concepts appears to be necessary in order to ensure that all the tissue included in the target volume receive the appropriate dose. For example: 1) The target volume can move(e.g. to reference bony structures) due to patient breathing. 2) The size and shape of the target volume can change(e.g. stomach, bladder). 3) The inaccuracy of patient and/or beam positioning has to be taken into account.

To account for these factors, the volumes "Gross Tumor Volume", "Clinical Target Volume" and "Planning Target Volume" have been proposed by the ICRU Working Group. GTV is the gross palpable or visible/demonstrable extent and location of the malignant growth. CTV is a tissue volume that contains a GTV and/or subclinical microscopic malignant disease, which has to be treated. The CTV is thus an anatomical-clinical concept that has to be defined before a choice of treatment modality and technique is made.

For 3D CRT, margins have to be added around the CTV to compensate for the effects of organ and patient movements and inaccuracies in beam and patient set up. This leads to the concept of the Planning Target Volume(PTV). The PTV is a geometrical concept, and it is defined to select appropriate beam sizes and beam arrangements, taking into consideration the net effect of all the possible geometrical variations and inaccuracies in order to ensure that the prescribed dose is actually delivered to the CTV.

Principles of Conformal Radiation Therapy

3D conformal therapy is a mode of high precision therapy designed to conform

the high dose volume to the shape of the tumor in its entire 3D configuration. Multiple static coplanar and noncoplanar fields are used to focus the dose onto the tumor while maximally excluding normal tissues from the volume receiving high radiation doses.

Treatment Planning Optimization

Optimization can be applied to all plan parameters including beam parameters (size, position, wedge angle and orientation, filters, blocks and boluses, relative weight, energy) and fractionation parameters (dose per fraction, number of fractions and their distribution in time). however, this would be a very difficult and time consuming process. It has been shown that impressive results can be achieved even with the beam weights being the only optimized parameters.

There are two major components of any optimization systems: 1) the description of the plan goals (optimization model) and 2) the method of achieving the desired goal (optimization algorithm).

The optimization model is usually expressed in a form of the objective(score) function which describes a figure of merit of a particular plan and is to be maximized or minimized, and/or a set of constraints(requirements) which have to be satisfied by the optimal plan and which define the domain of all feasible solutions.

The following have been investigated and judged to be clinically useful as objective functions or components of the objective function: 1) TCP, 2) NTCP, 3) the maximum or minimum dose a volume or given proportion of the volume, 4) the volume receiving dose smaller or larger than a certain limit, 5) the range of doses to the target volume, 6) the maximum/ minimum/ mean/ integral dose to a region of interest.

The optimization algorithm searches the domain of plan variables to find the optimal plan, that is the set of plan variables parameters such as beam weight, beam angles, field size and shape etc.) which maximize/minimize the chosen score function subject to constraints. A variety of optimization algorithms have been developed and those applied to treatment plan optimization can be grouped into the following categories: 1) exhaustive search techniques 2) linear, quadratic, and non-linear mathematical programming 3) finding a feasible solution 4) inverse solution approach 5) heuristic algorithms 6) artificial intelligence.

Quality Assurance for Treatment Planning of Conformal Therapy

Quality assurance for the treatment planning and delivery process is a very important part of high quality radiation oncology patient care. "Quality assurance for the treatment planning" has often been taken to refer to a limited number of activities centered around verifying that the planning system's calculated dose distributions were in reasonable agreement with data measured in a limited number of situations. Image-based anatomy and target definition, conformal beam shaping, 3-D dose calculations, plan evaluation tools, and plan verification data are now all part of the planning process. In the context of the expanded scope of treatment planning, quality assurance efforts must also be expanded to cover the above-described functions.

1. Quality Assurance for Treatment Planning Software

The quality and quality assurance of the software used for treatment planning is of course a critical part of the quality assurance process, the QA of this software is typically not under the control of the clinical user. For commercial vendors, there are various regulations and good manufacturing code practices, but even these factors are hampered by the lack of standards from the radiotherapy community about technically how these practices should be implemented in a practical way.

2. Dosimetric Quality Assurance

Calculation verification checks and quality assurance of dose calculations generated by treatment planning systems have always been the subject of QA.

1) Measured Dataset

Measurement of a complete and self-consistent three-dimensional dataset for each beam is critical. Although there are a few different methodologies for these measurements, we have used a film-based method.

2) Dose Distribution Comparison and Verification Techniques

To perform quantitative comparisons of data and calculations in 3D, direct overlays of 1D profiles and depth doses or perhaps 2D isodose curve plots are no longer adequate. A more effective method is to use subtraction of 3D measured and calculated distributions to generate a dose difference.

3) Verification of Input Data

The first step in the verification of the dose calculations is to verify the acc

uracy with which the algorithm reproduces the input data.

4) Study of the Applicability and Limits of the Dose Calculation Algorithm

The limits of usefulness of the dose calculation algorithm must be investigated and documented before it is clinically used.

5) Verification of the Calculations over the Range of Clinical Use

The accuracy of the dose calculations over the entire range of clinical uses should be documented.

6) Absolute Dose Output and Plan Normalization

One of the most critical parts of the entire treatment planning and treatment delivery process is the determination of the absolute dose and monitor units used to actually deliver the treatment to the patient. In 3D planning, the process involving beam normalization, dose prescription definition and monitor unit calculations must be verified.

Non-Dosimetric Quality Assurance

Another major segment of planning system QA involves the non-dosimetric parts of the planning process, including:

Image conversion	Dose Volume Histograms
Anatomical structure definition	Plan evaluation tools
Dataset registration	Plan verification tools
Density representation	Measured dose distribution tools
Image use	Composite plans
Anatomical display	Hard copy output
Beam/block/MLC/compensator definition	Absolute dose
Dose calculation grids, logic, etc.	Clinical system tests
Dose Display	

QA for the Entire Clinical Planning/Treatment Process

Some of the most important features of an extensive QA program for 3D treatment planning involve the use of checks and balances which are not built in to the treatment planning system, but rather are part of the routine treatment planning and treatment delivery process within the department.